

Temperature profiles of 980- and 1,470-nm endovenous laser ablation, endovenous radiofrequency ablation and endovenous steam ablation

W. S. J. Malskat · M. A. L. Stokbroekx · C. W. M. van der Geld ·
T. E. C. Nijsten · R. R. van den Bos

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Abstract Endovenous thermal ablation (EVTA) techniques are very effective for the treatment of varicose veins, but their exact working mechanism is still not well documented. The lack of knowledge of mechanistic properties has led to a variety of EVTA protocols and a commercially driven dissemination of new or modified techniques without robust scientific evidence. The aim of this study is to compare temperature profiles of 980- and 1,470-nm endovenous laser ablation (EVLA), segmental radiofrequency ablation (RFA), and endovenous steam ablation (EVSA). In an experimental setting, temperature measurements were performed using thermocouples; raw potato was used to mimic a vein wall. Two laser wavelengths (980 and 1,470 nm) were used with tulip-tip fibers and 1,470 nm also with a radial-emitting fiber. Different powers and pullback speeds were used to achieve fluences of 30, 60, and 90 J/cm. For segmental RFA, 1 cycle of 20 s was analyzed. EVSA was performed with two and three pulses of steam per centimeter. Maximum temperature increase, time span of relevant temperature increase, and area under the curve of the time of relevant temperature increase were measured. In all EVLA settings, temperatures increased and decreased rapidly. High fluence is associated with significantly higher temperatures and increased time span of temperature rise. Temperature profiles of 980- and 1,470-nm EVLA with tulip-tip fibers did not differ significantly. Radial

EVLA showed significantly higher maximum temperatures than tulip-tip EVLA. EVSA resulted in mild peak temperatures for longer durations than EVLA. Maximum temperatures with three pulses per centimeter were significantly higher than with two pulses. RFA temperature rises were relatively mild, resulting in a plateau-shaped temperature profile, similar to EVSA. Temperature increase during EVLA is fast with a high-peak temperature for a short time, where EVSA and RFA have longer plateau phases and lower maximum temperatures.

Keywords Endovenous thermal ablation · Varicose veins · Temperature profiles

Introduction

Endovenous thermal ablation (EVTA) techniques are nowadays commonly used as minimally invasive therapy for saphenous varicose veins. In comparison to surgical stripping or ultrasound-guided foam sclerotherapy, endovenous laser ablation (EVLA) and radiofrequency ablation (RFA) are proven to have a higher success rate and lower complication rate [1]. The efficacy safety of endovenous steam ablation (EVSA) for varicose veins has been shown in sheep and humans in a pilot study [2].

Although EVTA (EVLA, RFA, and EVSA) treatments are very effective, the exact working mechanism is not well documented, especially of EVLA, of which temperature profiles and its determinants (e.g., power, wavelength, type of fiber tip, and pullback speed) are not well studied. It is generally thought that thermal injury to the venous wall is responsible for vein occlusion in EVTA treatments [3–6]. Recently, we performed endovenous-simulated laser experiments showing no difference in the temperature profile between 940- and 1,470-nm lasers suggesting wavelength-independent temperature

W. S. J. Malskat (✉) · M. A. L. Stokbroekx · T. E. C. Nijsten ·
R. R. van den Bos (✉)
Department of Dermatology, Erasmus Medical Center,
Burgemeester's Jacobsplein 51, 3015, CA Rotterdam,
The Netherlands
e-mail: w.malskat@erasmusmc.nl
e-mail: r.vandenbos@erasmusmc.nl

C. W. M. van der Geld
Department of Mechanical Engineering, Eindhoven University
of Technology, Eindhoven, The Netherlands

profiles [7]. Also, experimental temperature measurements in EVSA demonstrated a dose–response relationship of heat induction of one, two, and three pulses of steam per centimeter [8]. However, comparison of temperature profiles between the different EVTA treatments (i.e., EVLA, RFA, and EVSA) in the same experimental setting has never been performed.

The lack of knowledge of mechanistic properties in EVTA treatments has led to a variety of EVTA protocols and a commercially driven dissemination of new or modified techniques without robust scientific evidence. Therefore, we compared the temperature profiles (maximum temperature, seconds of heating >50 °C and area under the curve of the maximum temperature set against the time) of 980- and 1,470-nm EVLA, segmental RFA and EVSA in an experimental setting, simulating clinical conditions to assess differences in their main working mechanisms (i.e. heating of veins).

Methods

The experimental set-up (Fig. 1) consisted of a transparent plastic box, in which a poly vinyl chloride (PVC) tube was fixed. The tube was filled with 30-mm diameter cylinders of raw potato, to mimic a vein. Raw potato was chosen because it has a solid structure, consists of 80 % water (which is similar to a vein wall), is relatively stable under high temperatures, and can be cut. These cylinders had a 2.4-mm diameter hole in the center, in which the laser fiber, radiofrequency, or steam catheter was inserted. The box was filled with heparinized pig blood. The temperature measurements were performed with five 0.5-mm K-type thermocouples (TC; Omega KMQSS-IM050G-150) connected to a data sampler (Omega, Pico TC08). Five TCs were positioned within the PVC tube (TC 1, 2, 3, 4, 5) at three different distances from the fiber (TC 1 and 5 at 0 mm, TC 2 and 4 at 1 mm, TC 3 at 2 mm), because it was hypothesized that the temperature profiles would differ for various positions due to heat development by the moving fiber. The thermocouples were fixed on a sliding block, inserting and positioning the TCs for each experiment.

The EVLA, RFA, and EVSA devices used and their settings were similar to clinical practice [2, 9]. Two laser wavelengths were used as follows: 980-nm Diode (Quanta System, Solbiate Olona, VA, Italy) and 1,470-nm Biolitec, ELVeS (Quanta System, Solbiate Olona, VA, Italy) with tulip-tip fibers [10] (Tobrix, Waalre, The Netherlands) and 1,470 nm also with a radial-emitting fiber [11] (Tobrix, Waalre, The Netherlands). A tulip-tip is an umbrella-like cover that centers the laser fiber in the vein (diameter 600 μ m). A radial-emitting fiber emits the laser light perpendicular to the fiber (diameter 2 mm). For steam ablation, the Steam Vein Sclerosis system (CERMA S.A., Archamps, France) was used (fiber diameter 1.2 mm). For RFA, a segmental heating catheter of 7F (2.3 mm) diameter (ClosureFast catheter, VNUS Medical

Technologies Inc, San Jose, California) with a 7-cm heating element was used.

For EVLA, six pullback speeds (0.5, 1, 1.5, 2, 3, and 4 mm/s), were combined with different laser settings (varying from 3 to 12 W for both wavelengths), achieving linear endovenous energy densities (LEED) of 30, 60, and 90 J/cm. In order to reach accurate and constant pullback speeds, a linear motor with frequency regulator was used. For segmental RFA, temperature experiments were done with 1 cycle of 20 s. EVSA was performed with two and three pulses of steam per centimeter, separately. Every measurement was repeated 5 times, which resulted in 10 measuring points at 0 and 1 mm and 5 at 2-mm distance from the fiber.

To study the temperature profiles, dT_{max} , dt , and $dtdT$ were calculated from the graphical representation. Here, dT_{max} was defined as the maximum temperature increase above room temperature (20 °C). Maximum temperatures above 50 °C (thus an increase of 30 °C above room temperature) were considered relevant, since it is the assumed threshold for collagen denaturation needed to irreversibly damage the vein wall [12–14]. Parameter dt was defined as the time span that the temperature increase was relevant (duration of $dT_{max} >30$ °C). Parameter $dtdT$ represents the area under the curve of the time that the temperature increase was more than 30 °C.

Statistical analyses

The three continuous temperature measures (dT_{max} , dt , and $dtdT$) are presented as means with a standard deviation (SD). We used SPSS 15.0 software (SPSS Inc, Chicago, IL) for the analyses. The comparison of these measures between the different settings of each EVLA device was done by ANOVA testing. Independent T tests were performed to compare different EVLA wavelengths (980 and 1,470 nm), different EVLA fiber tips (tulip and radial), and two and three pulses of EVSA. Two-sided p values were considered to be significant if <0.05 .

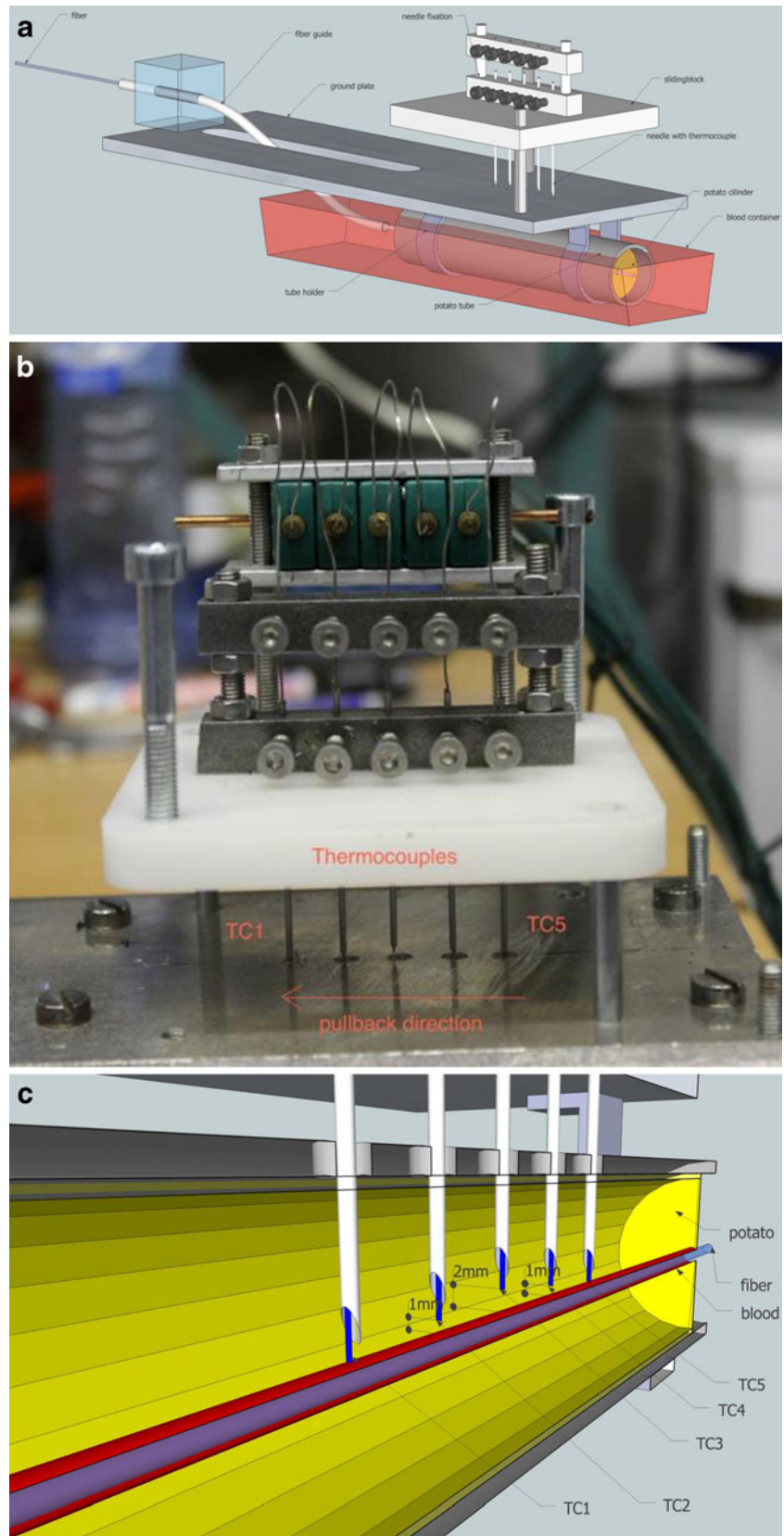
Results

EVLA

Table 1 shows the results of dT_{max} at 0 mm, dt and $dtdT$ for 980- and 1,470-nm tulip and 1,470-nm radial EVLA. Temperature profiles of EVLA tulip 980 and 1,470 nm are depicted in Figs. 2 and 3.

Temperature profiles of 980- and 1,470-nm EVLA were measured with tulip-tip and radial fibers, with levels of energy varying from 30 to 90 J/cm. In all EVLA settings, the temperature rise peaked and decreased rapidly. In all settings, dT_{max} was at least 30 °C ($T_{max} \geq 50$ °C) at 0-mm distance

Fig. 1 **a.** Schematic reproduction of the experimental setting. **b.** Detail of sliding block with thermocouples (*TC1* thermocouple 1; *TC5* thermocouple 5). **c** Cross-section of potato with position of thermocouples (*TC2* thermocouple 2; *TC3* thermocouple 3; *TC4* thermocouple 4) in relation to the fiber/catheter. *TC2*, *TC3*, and *TC4* are positioned inside the potato “wall”



from the fiber tip. At 1-mm distance, most values of dT_{max} were below 30 °C. At 2-mm distance, none of the settings

exceeded a dT_{max} of 30 °C. In most settings, dt is more than 5 s. The results will be listed in detail below.

Table 1 EVLA measurements

	980 nm [#]			1,470 nm ^{#S}			1,470 nm ^S		
	Tulip fiber			Tulip fiber			Radial fiber		
	30 J/cm*	60 J/cm*	90 J/cm*	30 J/cm*	60 J/cm*	90 J/cm*	30 J/cm*	60 J/cm*	90 J/cm*
dTmax 0 mm (mean ± SD)	49±4	51±7	65±10	48±8	59±19	60±12	68±14	87±16	94±7
dt (mean ± SD)	4±1	13±3	22±8	5±2	15±6	30±5	5±1	18±4	26±0
dtdT (mean ± SD)	193±30	563±136	1,291±281	220±66	843±316	1,431±306	236±74	912±203	1,465±37

dTmax maximum temperature increase in degrees Celsius (°C) above room temperature (20 °C); SD standard deviation; dt duration of dTmax >30 °C in seconds (s); dtdT area under the curve (°C × s) of the time that the temperature increase is >30 °C

*Statistical comparisons of dTmax, dt, and dtdT between the three fluence rates (30, 60, and 90 J/cm) of each device (980 and 1,470-nm tulip fiber and 1,470-nm radial fiber) were highly significant (ANOVA; $p < 0.001$, except for dTmax of 1,470-nm tulip fiber $p = 0.03$)

[#] Differences in the distribution of dTmax, dt, and dtdT between 980 and 1,470-nm tulip fiber lasers were not significant (Independent T test; $p = 0.82$, 0.10, and 0.18, respectively)

^S dTmax was significantly higher for 1,470-nm radial fiber compared to 1,470-nm tulip fiber (Independent T test; $p < 0.001$) whereas dt and dtdT were comparable (Independent T test; $p = 0.11$ and $p = 0.20$, respectively)

LEED

A higher total level of delivered energy per centimeter vein length, resulting from a relatively high power and/or a lower pullback speed, generated a higher dTmax at 0 mm in all EVLA devices. A dt <5 s seemed to be associated with a relatively low total level of energy per centimeter vein length (30 J/cm).

Statistical comparison of dTmax, dt, and dtdT between 30, 60, and 90 J/cm of each device (980- and 1,470-nm tulip fiber and 1,470-nm radial fiber), were highly significant (ANOVA; $p < 0.001$, except for dTmax of 1,470-nm tulip fiber $p = 0.03$), indicating an increasing dTmax at 0 mm, dt, and dtdT at higher LEED.

Wavelengths

The p values of dTmax 0 mm, dt, and dtdT were not significantly different between 980 and 1,470 wavelengths

(Independent T test; $p = 0.82$, 0.10, and 0.18, respectively). Temperature profiles of 980- and 1,470-nm EVLA were comparable.

Fiber tips

For 1,470-nm EVLA, dTmax at 0 mm was significantly higher for the radial fiber than for the tulip-tip fiber (Independent T test; $p < 0.001$). However, dt and dtdT were comparable (independent T test; $p = 0.11$ and 0.20, respectively).

EVSA

In Table 2, results are presented of dTmax at 0 mm, dt, and dtdT for two and three pulses of steam. Temperature profile of EVSA is shown in Fig. 4.

Temperature curves of EVSA showed a plateau phase, with a relatively constant temperature for a longer period of time.

Fig. 2 Temperature profile of 980-nm tulip EVLA. dTmax maximum temperature increase above room temperature (20 °C); TC1 thermocouple 1; TC2 thermocouple 2; TC3 thermocouple 3; TC4 thermocouple 4; TC5 thermocouple 5

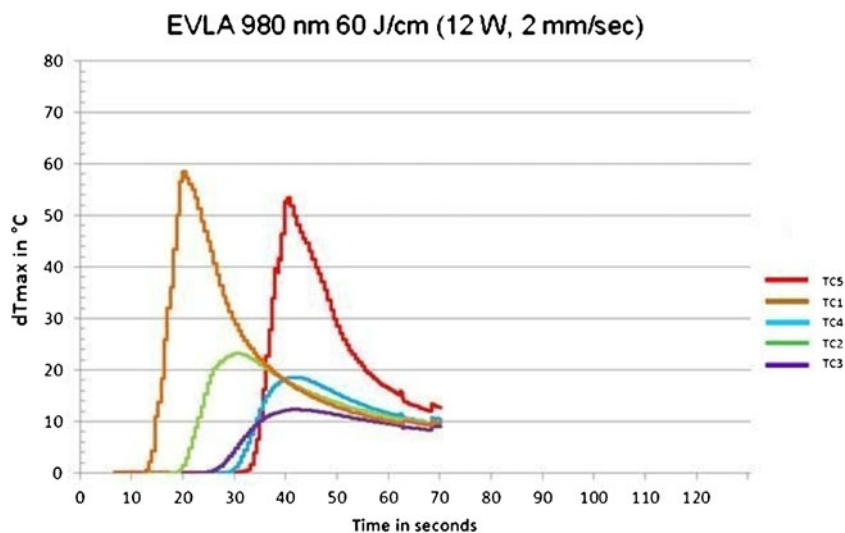
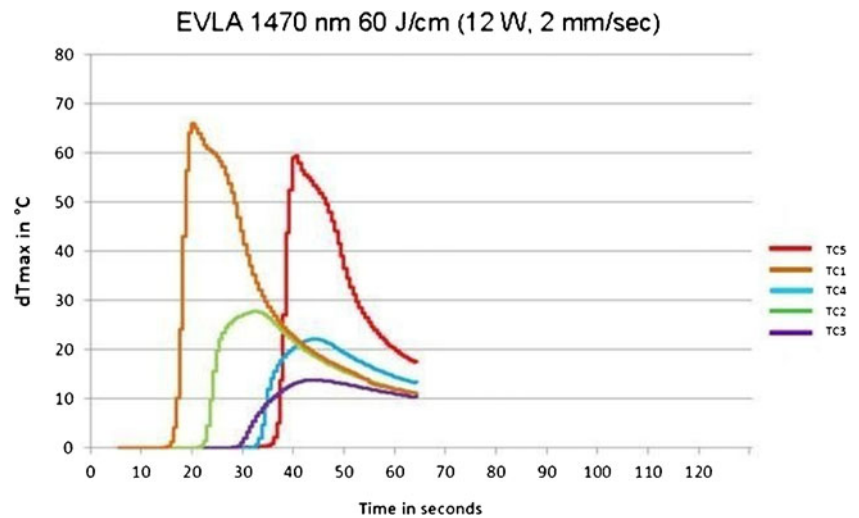


Fig. 3 Temperature profile of 1, 470-nm tulip EVLA. dT_{max} maximum temperature increase above room temperature (20 °C); *TC1* thermocouple 1; *TC2* thermocouple 2; *TC3* thermocouple 3; *TC4* thermocouple 4; *TC5* thermocouple 5



With two and three pulses of steam per centimeter, dT_{max} was over 30 °C at 0-mm distance of the EVSA catheter. At 1- and 2-mm distance, dT_{max} was below this cut-off point. dT_{max} at 0 mm was significantly higher with three pulses of steam, than with two pulses (independent *T* test; $p=0.024$). A significant difference was also found in *dt*; with two pulses per centimeter, *dt* was significantly lower than with three pulses (independent *T* test; $p<0.001$), but both had a mean $dt>5$ s.

RFA

Table 2 shows results of dT_{max} at 0 mm, *dt*, and *dtdT* for RFA. Temperature profile of RFA is depicted in Fig. 5.

Temperature curves of segmental RFA showed a plateau phase, with a relatively constant temperature for a longer period of time. dT_{max} was over 30 °C at 0-mm distance of the RFA catheter. At 1- and 2-mm distance, dT_{max} was below this cut-off point for both measurements. Also, *dt* was >5 s.

Comparison of EVTAs

For both EVSA and segmental RFA, temperature curves showed a plateau phase, with a relatively constant temperature for a longer period of time, whereas for EVLA, the temperature peaked and decreased more rapidly with less of a plateau phase. Also, the settings of EVLA in high LEED 90 J/cm, generated a higher dT_{max} , than RFA and EVSA. However, all devices were comparable in achieving a sufficient dT_{max} over 30 °C at fiber or catheter level, and a $dt >5$ s. All EVTA devices could induce an adequate temperature rise at the fiber or catheter level and they all led to a long enough time span at the temperature needed for collagen denaturation.

Discussion

This is the first experimental study that showed temperature profiles of EVLA for different wavelengths with tulip and radial fiber tips, EVSA, and segmental RFA. This study allowed us to compare temperature profiles of most of the available different endovenous thermal therapies, used in patients with varicose veins.

The results of these temperature measurements showed several interesting characteristics. We will discuss the results per device.

EVLA

The temperature rise of EVLA increased with higher LEED. Temperature behavior of EVLA was different compared to EVSA or segmental RFA; the peak temperature was higher for a shorter time. Possibly, high peak temperatures may result in vein wall perforation and/or more perivenous damage,

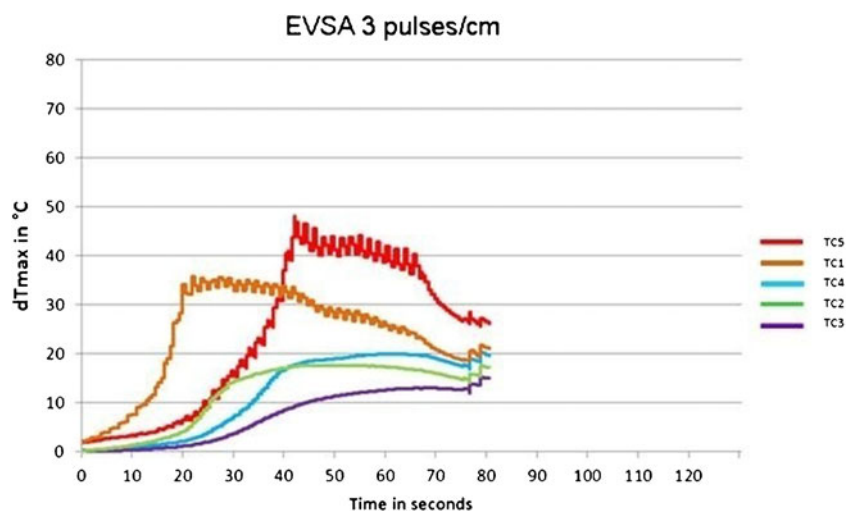
Table 2 RFA and EVSA measurements

	RFA	EVSA	
		1 cycle	2 pulses*
dT_{max} 0 mm (mean \pm SD)	39 \pm 11	43 \pm 3	52 \pm 7
<i>dt</i> (mean \pm SD)	14 \pm 9	17 \pm 1	32 \pm 2
<i>dtdT</i> (mean \pm SD)	524 \pm 318	583 \pm 40	1,308 \pm 152

dT_{max} maximum temperature increase in degrees Celsius (°C) above room temperature (20 °C); *SD* standard deviation; *dt* duration of $dT_{max}>30$ °C in seconds (s); *dtdT* area under the curve (°C \times s) of the time that the temperature increase is >30 °C

*Statistical comparisons of dT_{max} 0 mm, *dt*, and *dtdT* between two and three pulses of steam were significant (Independent *T* test, $p=0.02$, <0.001 , and <0.001 , respectively)

Fig. 4 Temperature profile of EVSA. dT_{max} maximum temperature increase above room temperature ($20\text{ }^{\circ}\text{C}$); *TC1* thermocouple 1; *TC2* thermocouple 2; *TC3* thermocouple 3; *TC4* thermocouple 4; *TC5* thermocouple 5



causing (minor) side effects such as pain and ecchymoses, which seemed to occur more often in EVLA than in segmental RFA [15].

Temperature profiles of 980- and 1,470-nm with tulip-tip fibers did not differ significantly, which was in agreement with our previous findings [7]. High LEED, on the other hand, was again proven to be associated with significantly higher temperatures and increased time span of temperature rise compared to lower LEED. It is likely that the alleged differences in side effect profiles between different wavelengths, as described in previous studies, were the result of differences in administered joule per centimeter [16], power [17], or laser tip design [18], rather than difference in wavelength.

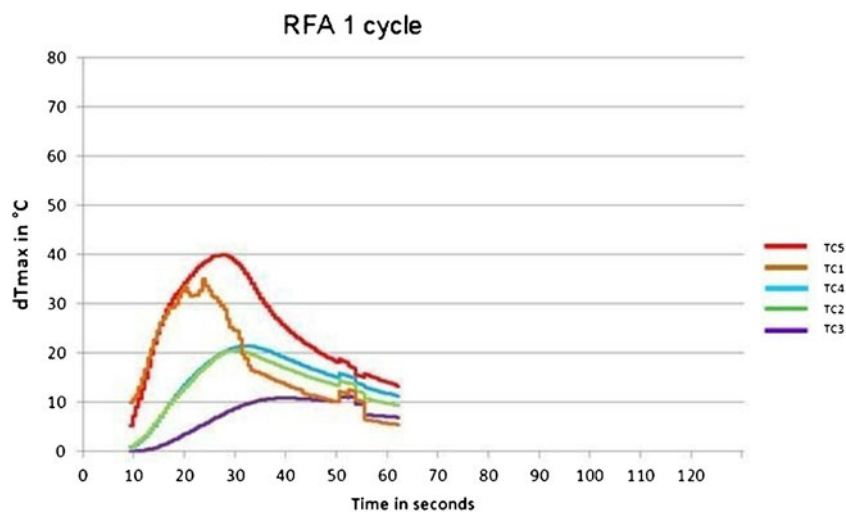
Radial 1,470-nm EVLA resulted in a significantly higher dT_{max} at 0 mm than tulip 1,470 nm EVLA, but a comparable temperature profile with a peak-shaped curve. The most likely explanation for the significant difference in dT_{max} is that radial fibers have a larger diameter than bare fibers and are therefore closer to the thermocouples. Also, direct absorption of the laser light by the thermocouples could be an explanation

for higher temperature measurements. In an additional experiment, we tested that direct irradiation of the thermocouple by the radial fiber resulted in barely any temperature rise, so direct emittance can be excluded as possible explanation for the difference.

EVSA

The dT_{max} of EVSA with three pulses per centimeter was significantly higher than with two pulses. Also, dt and $dtdT$ were larger for EVSA with three pulses per centimeter. This outcome is in line with previously reported temperature measurements which led to the recommendation of administering two or more pulses per centimeter in human veins [8]. EVSA resulted in mild peak temperatures for longer duration than EVLA, which was graphically shown as a long plateau phase. This implicated a longer homogeneous temperature rise of the vein wall, compared to EVLA, and could possibly result in a milder side effect profile, similar to segmental RFA. A clinical randomized trial should assess this possible difference.

Fig. 5 Temperature profile of segmental RFA. dT_{max} maximum temperature increase above room temperature ($20\text{ }^{\circ}\text{C}$); *TC1* thermocouple 1; *TC2* thermocouple 2; *TC3* thermocouple 3; *TC4* thermocouple 4; *TC5* thermocouple 5



Segmental RFA

Segmental RFA temperatures were measured for the standard setting (1 cycle). The catheter of segmental RFA was 2.2 mm in diameter, and was therefore closer to the thermocouples than the other devices. However, this did not lead to significantly higher temperature measurements at catheter level. The temperature rise was relatively mild; comparable to EVSA and lower than EVLA. Parameter dt was >5 s. This also resulted in a plateau-shaped temperature profile, similar to EVSA. Segmental RFA values of dt and dt/dT in our experiment were comparable to EVLA tulip tip 980- and 1,470-nm at 60 J/cm. This is in line with the reported 68.2 J/cm as described by Proebstle et al. [19]. The energy level of 1 cycle segmental RFA seemed to correlate with 60 J/cm EVLA, but the temperature profile was different because of the lack of peak temperature in segmental RFA. The absence of a peak temperature could be the explanation of the milder side effect profile of RFA, compared to EVLA [15].

Conclusion

In conclusion, temperature rises during EVLA are fast with a high-peak temperature for a short time, whereas EVSA and RFA have longer plateau phases and lower maximum temperatures. Temperature profiles of 940/980 and 1,470-nm EVLA are again shown to be similar [7]. Overall, differences in temperature levels of endovenous thermal ablation techniques are now proven to be minimal. The studied temperature profiles suggest that in clinical practice, all three EVTA methods will result in sufficient heating to obliterate the targeted vein, with more minor side effects (pain, ecchymoses) in EVLA, due to higher maximum temperatures.

References

- van den Bos R, Arends L, Kockaert M, Neumann M, Nijsten T (2009) Endovenous therapies of lower extremity varicosities: a meta-analysis. *J Vasc Surg* 49:230–9
- van den Bos RR, Milleret R, Neumann M, Nijsten T (2010) Proof-of-principle study of steam ablation as novel thermal therapy for saphenous varicose veins. *J Vasc Surg* 53:181–6
- Mordon SR, Wassmer B, Reynaud JP, Zemmouri J (2008) Mathematical modeling of laser lipolysis. *Biomed Eng Online* 7:10
- Proebstle TM, Sandhofer M, Kargl A et al (2002) Thermal damage of the inner vein wall during endovenous laser treatment: key role of energy absorption by intravascular blood. *Dermatol Surg* 28:596–600
- Fan CM, Rox-Anderson R (2008) Endovenous laser ablation: mechanism of action. *Phlebology* 23:206–13
- Mordon SR, Wassmer B, Zemmouri J (2006) Mathematical modeling of endovenous laser treatment (ELT). *Biomed Eng Online* 5:26
- van den Bos RR, van Ruijven PW, van der Geld CW, van Gemert MJ, Neumann HA, Nijsten T (2012) Endovenous simulated laser experiments at 940 nm and 1470 nm suggest wavelength-independent temperature profiles. *Eur J Vasc Endovasc Surg* 44:77–81
- van Ruijven PW, van den Bos RR, Alazard LM, van der Geld CW, Nijsten T (2011) Temperature measurements for dose-finding in steam ablation. *J Vasc Surg* 53:1454–6
- Nijsten T, van den Bos RR, Goldman MP et al (2009) Minimally invasive techniques in the treatment of saphenous varicose veins. *J Am Acad Dermatol* 60:110–9
- Vuylsteke M, Van Dorpe J, Roelens J, De Bo T, Mordon S, Fourneau I (2010) Intraluminal fibre-tip centring can improve endovenous laser ablation: a histological study. *Eur J Vasc Endovasc Surg* 40:110–6
- Pannier F, Rabe E, Rits J, Kadiss A, Maurins U (2011) Endovenous laser ablation of great saphenous veins using a 1470 nm diode laser and the radial fibre—follow-up after six months. *Phlebology* 26:35–9
- Biesman BS, Khan J (2000) Laser incisional surgery. *Clin Plast Surg* 27(2):213–220
- Moritz AR, Henriques FC (1947) Studies of thermal injury: II. The relative importance of time and surface temperature in the causation of cutaneous burns. *Am J Pathol* 23:695–720
- Vangsness CT Jr, Mitchell W III, Nimmi M, Erlich M, Saadat V, Schmotzer H (1997) Collagen shortening. An experimental approach with heat. *Clin Orthop Relat Res* 337:267–271
- Rasmussen LH, Lawaetz M, Bjoern L, Vennits B, Blemings A, Eklof B (2011) Randomized clinical trial comparing endovenous laser ablation, radiofrequency ablation, foam sclerotherapy and surgical stripping for great saphenous varicose veins. *Br J Surg* 98:1079–87
- Almeida J, Mackay E, Javier J, Mauriello J, Raines J (2009) Saphenous laser ablation at 1470 nm targets the vein wall, not blood. *Vasc Endovascular Surg* 43:467–72
- Proebstle TM, Moehler T, Gul D, Herdemann S (2005) Endovenous treatment of the great saphenous vein using a 1,320 nm Nd:YAG laser causes fewer side effects than using a 940 nm diode laser. *Dermatol Surg* 31:1678–83, discussion 83–4
- Doganci S, Demirkilic U (2010) Comparison of 980 nm laser and bare-tip fibre with 1470 nm laser and radial fibre in the treatment of great saphenous vein varicosities: a prospective randomised clinical trial. *Eur J Vasc Endovasc Surg* 40:254–9
- Proebstle TM, Vago B, Alm J, Gockeritz O, Lebard C, Pichot O (2008) Treatment of the incompetent great saphenous vein by endovenous radiofrequency powered segmental thermal ablation: first clinical experience. *J Vasc Surg* 47:151–6